



# Linear Accelerator Technology



Dept of Radiotherapy & Radiation Medicine Institute of Medical Sciences Banaras Hindu University, Varanasi



### **Selection - Teletherapy Machine**

#### **Radiation Beam Characteristics**

 Beam edge sharpness (penumbra) , Beam penetration (energy)

#### **Machine Characteristics**

- **\*** Dose rate, Patient collimator distance
- Isocentre height, Radioactive source versus x-rays

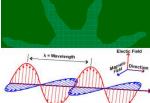
Service/Maintenance Issues

- **Safety Considerations**
- **\*** Radiation protection
- **Cost Considerations**

**Additional Features** 

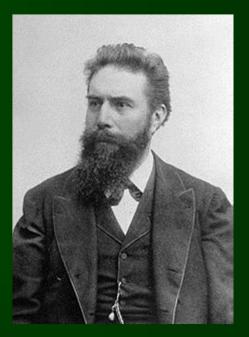


#### Introduction



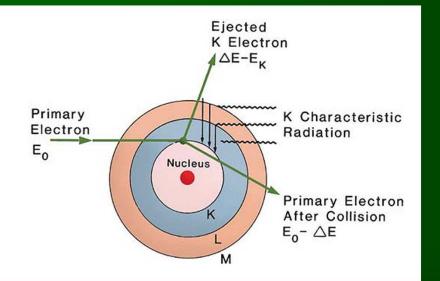


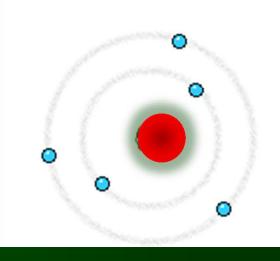
- What is Linac?
  - X-rays, Electron
- What is x-rays?
- Incidental discovery!
- How x-rays are produced?Physics of x-rays





## Characteristic X-rays

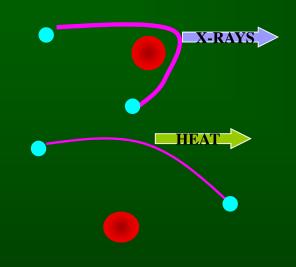


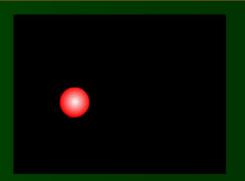


#### from Faiz Khan



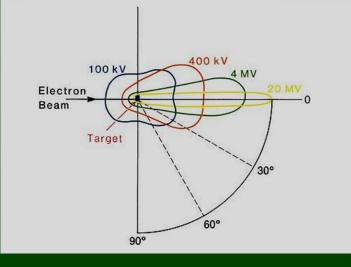
# Bremsstrahlung X-rays







#### **Angular Distribution**



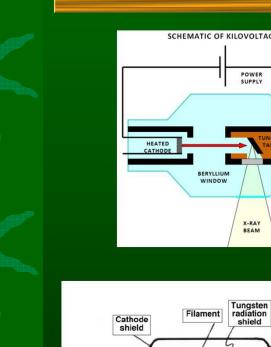
#### from Faiz Khan

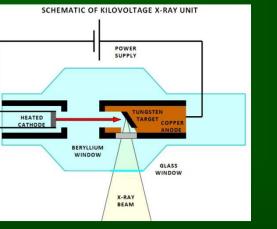
**P** 

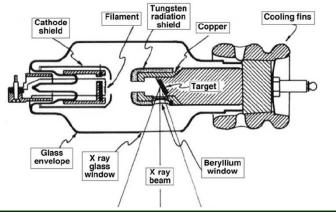
\* Angular distribution becomes more "forward peaked" as the electron energy increases

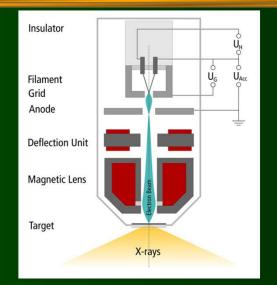


# X-Ray Tube

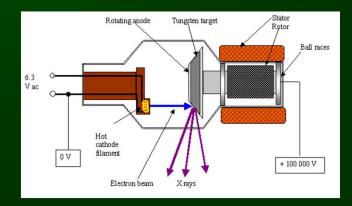








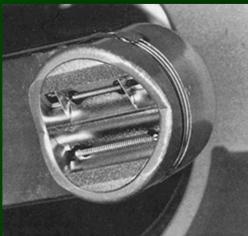
#### microfocus x-ray tubes (NDT)





#### Cathode

Tungsten filament (3370 ° C)
Thermionic emission
Focusing cup
Dual filaments





#### Anode

**\***Tungsten target

- High melting point
- High Z (74) , X-ray  $\alpha$  Z²
- **\***Heat dissipation
  - Copper anode
  - Rotating anode /Stationary



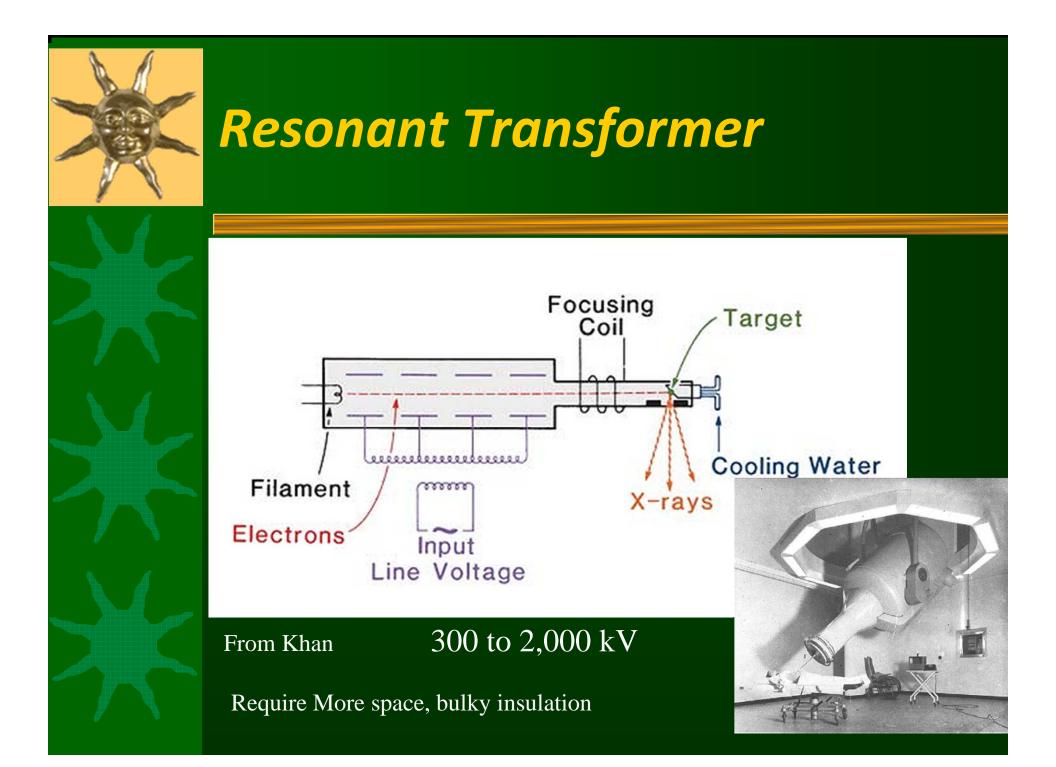
Anode hood – copper and tungsten shields intercept stray electrons and x rays



# Limitations of X-ray Tube

 High voltage
 Millions of volts cannot be held in single gap







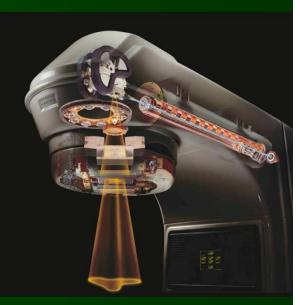
## **Clinical Radiation Generators**

★ Grenz rays	< 20 kVp
Contact Therapy	40-50 kVp
Superficial Therapy	50-150 kVp
Orthovoltage	150-500 kVp
★ Supervoltage	500-1000 kVp
★ Megavoltage	> 1000 kVp



#### Linac?

A device in which electron beam is accelerated in linear path with the help of high frequency microwaves to produces high energy photon or electron beam





#### **History**

# Linacs were developed concurrently by two groups:

- W.W. Hansen's group at Stanford University in the U.S.A.
- D.D. Fry's group at Telecommunications Research Establishment in the U.K.

\* Both groups - interested in Linacs for research

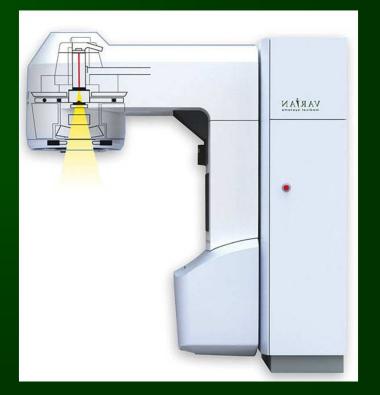
 Feasible - radar technology developed during World War II



#### **Basic Linac**

Low energy ★ 4-8 MV

- Straight-through beam
- No Bending
- fixed flattening filter
- external wedges
- symmetric jaws
- single ionisation chamber
- isocentric mounting.





# Medium/High Energy

#### **\***10-25 MV

- Dual photon energy and multiple electron energies
- Achromatic bending
- dual scattering foils or scanned electron pencil beam
- motorized wedge
- Asymmetric jaws.

#### \*Advanced features

- EPID, MLC
- IMRT, IGRT





#### **Basic Accelerator Technology**

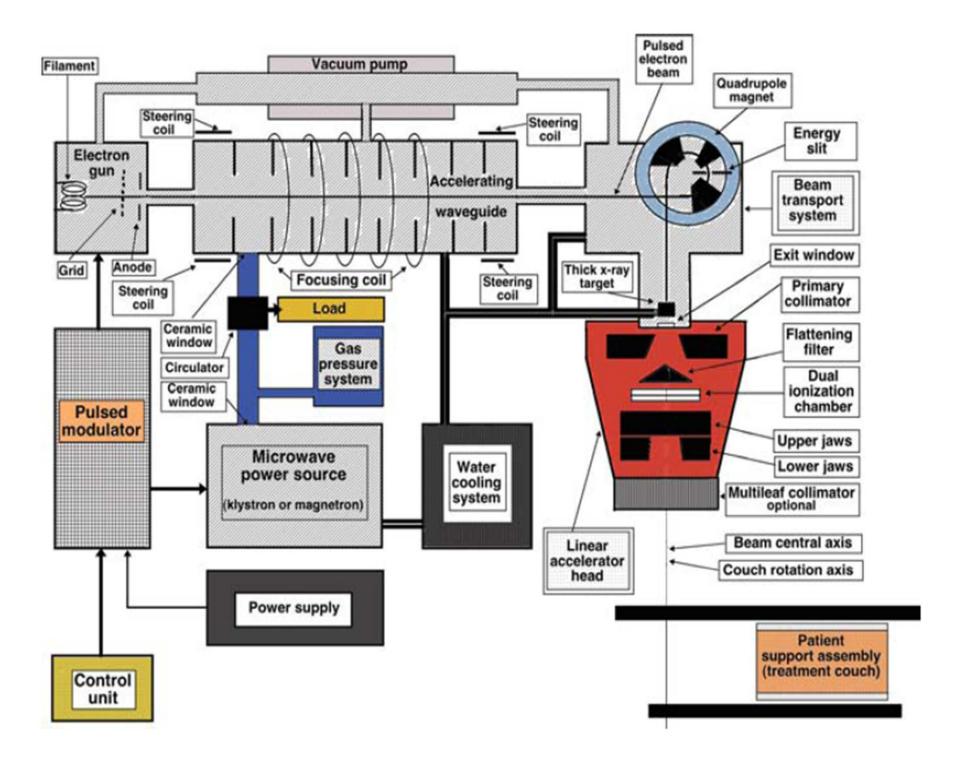
**\*** Sophisticated & complex **\*** Mechanical, Electrical, electronics, Radiation, Optics, **Microwave \*** Microwave Power sources **\*** Acceleration structures **\*** Beam transport systems **\*** Support structures





### **Major Components**

- ★ Control Console
- Power Supply
- ✤ Modulator
- ✤ Magnetron or Klystron
- ✤ Electron Gun
- ★ Wave Guide system
- ✤ Accelerator Tube
- ✤ Bending Magnet
- Treatment Head (Straight Beam/(Bent Beam)
- Treatment Couch



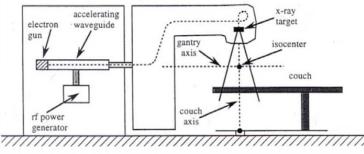


### **Modulator Cabinet**

The combination of high voltage source, PFN, HV switch, and pulse transformer is known as "modulator"

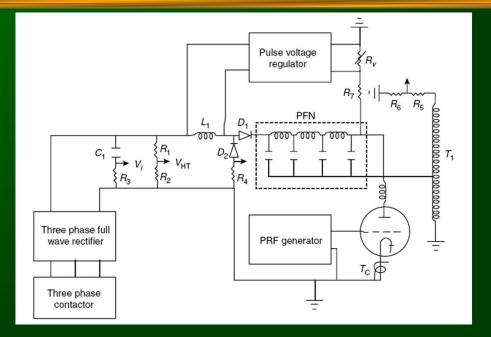
 Power distribution system
 High Voltage pulses to gun & RF Generator
 Power suppliers











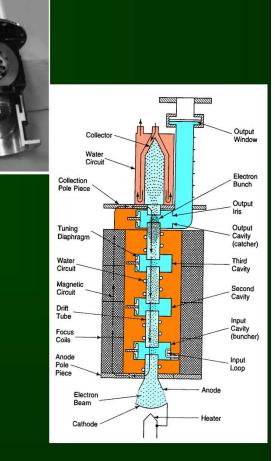
- The modulator supplies high-voltage pulses lasting a few microseconds to the microwave source and electron gun.
- The PRF (pulse repetition frequency) is set by the PRF generator connected to the thyratron grid and is usually adjustable in the range 50 Hz to 1000 Hz.



#### **Microwave Source**

#### **\*** Magnetron

- Low energy accelerators
- Less costly
- Smaller least complicated
- Less reliable
- shorter lifespan
- 🗡 Klystron
  - Stable at higher energies
  - Costly & Complex
  - Bulky





### **Classification as per RF fields**

#### **\star** L band - 10<sup>3</sup> MHz

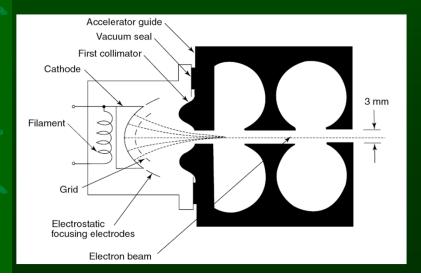
- physically larger but capable of beam powers considerably above 20 kW
- **\***S band 2856 MHz
  - more compact but limited to beam powers below 20 kW
- **\star** X band 10<sup>4</sup> MHz
  - Tomotherapy
  - robotic arm mounting, miniature form
  - Mobetron (IORT system)



#### **Electron Gun**

Source of the electrons
Produced thermionically
Injected onto the central axis of the waveguide.







## Vacuum & Cooling

#### \*The vacuum system

- Maintains required low pressures
- required for operation of WG, Gun and bending magnets.
- Prevents breakdown of the high electric fields required during accelerator operation.

#### \*The water cooling system

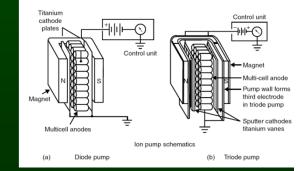
Required to establish a stable operating temperature.



#### Ion Pump

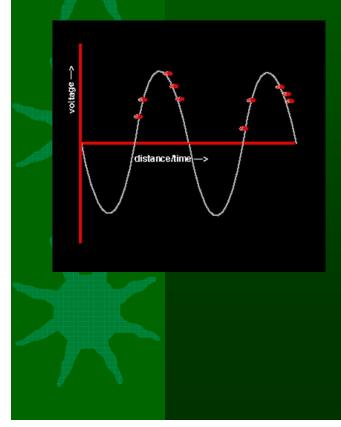
- Electric field to accelerate and traps ions
- Solid electrodes in pump usually made from Titanium.
- Ion Pumps have no moving parts and use no oil

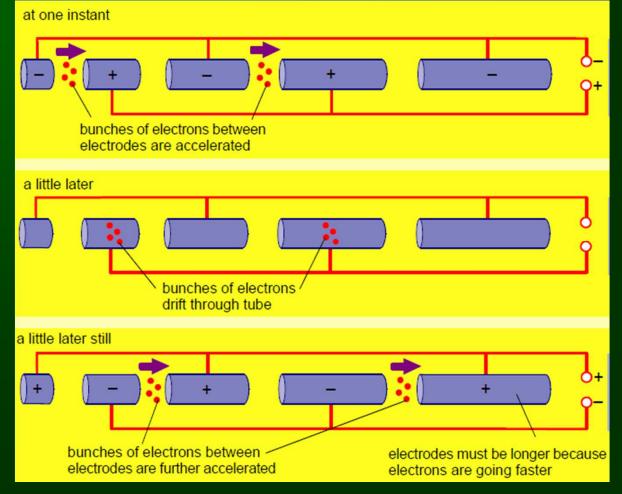






#### **Electron Acceleration**

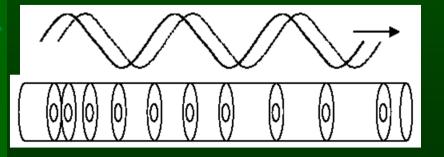




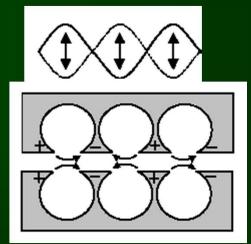


### **Accelerator Structures**

A cylindrical tube in which electrons from electron gun, are accelerated by the amplified microwaves and exit the waveguide to enter the *treatment head*.



**Travelling Wave** 



Standing Wave

Accelerator technique - © Sverker Werin, Max-lab 2000

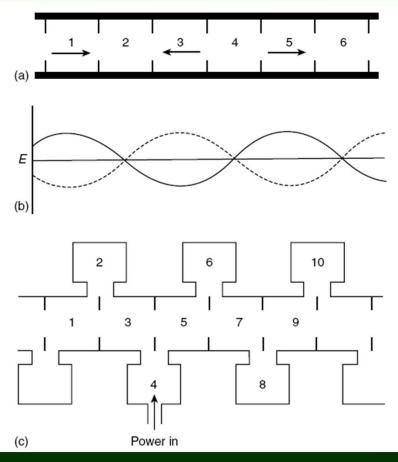


### Standing wave

(a) Arrangement of the waveguide.

(b) Standing waves.

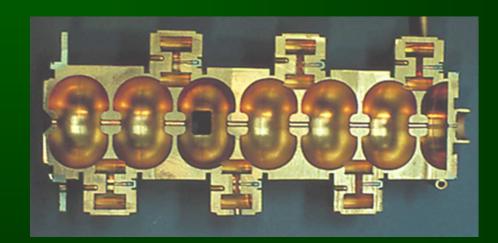
(c) Shows a side-coupled cavity.



From Greene and Williams



# Section of SW accelerator





#### Comparison

#### **Travelling Wave**

- Longer structure
- Short fill time
- Circulator not required
- High accelerating beam capacity
- Spectrum insensitive to accelerating field
- Bunching less sensitive to accelerating field
- Generally low vacuum requirement

#### **Standing Wave**

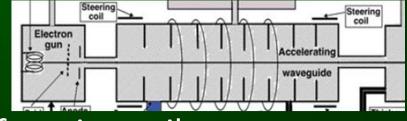
- \* Shorter structure
- ✤ Longer fill time
- Circulator required
- Low accelerating beam capacity
- Spectrum sensitive to accelerating field
- Bunching highly sensitive to accelerating field
- High vacuum requirement



#### Focusing

#### **\***Focusing coils

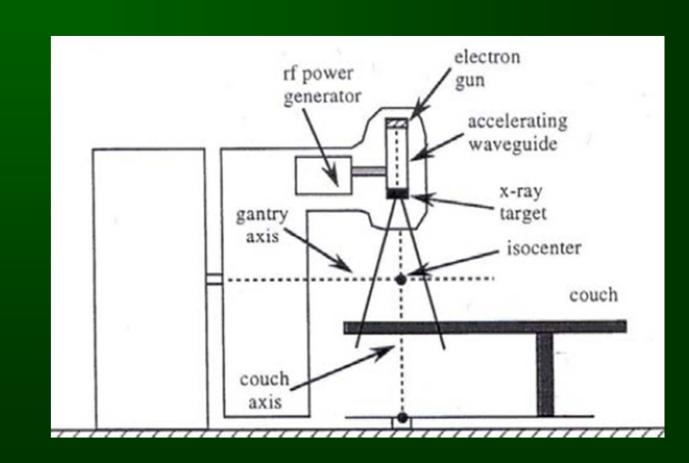
- Aligned along the exterior of the waveguide.
- Magnetic fields parallel to the long axis of the waveguide.
- Steering coils



- Independently of focusing coils
- Ensure, electron beam is at the centre of WG
- Entrance and exit electron beam as desired



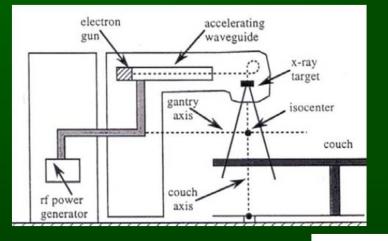
### **Position of WG**



#### Wave guide in Head

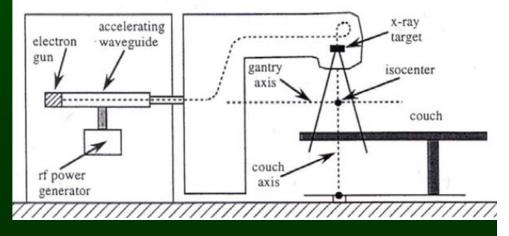


### Position of WG



#### Wave guide Gantry

Wave guide in Gantry Stand

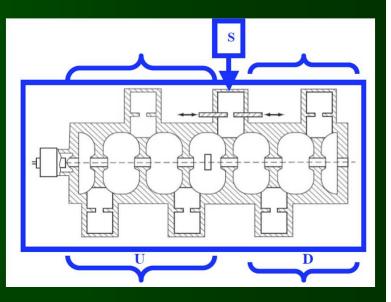




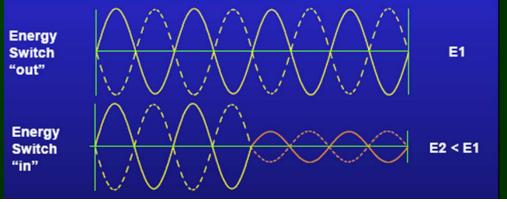
### **Energy Change?**

#### \* Energy switch

 fields in the accelerating cavities in section D may be varied in a controlled amount relative to the fields in the cavities in section U



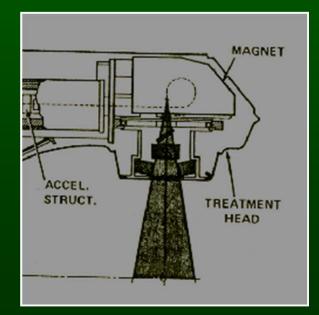
Video

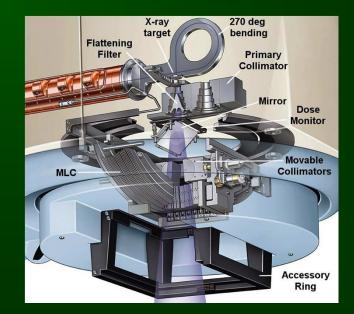




#### **Treatment Head**

# Contains the beam shaping, steering, and control components of the linear accelerator.







#### **Components in Head**

Scattering Foils –to spread the beam
Monitoring Chambers – to monitor
Collimation System – fixed and movable
X-Ray Target – transmission-type
Flattening Filter –to produce a "flat" beam



#### Bending magnet

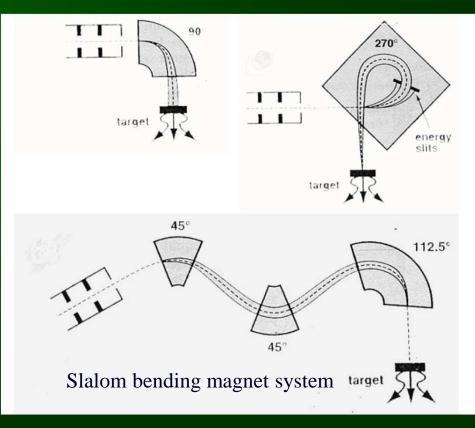
#### **\***projects the electron beam onto the

#### target.

90<sup>0</sup> - Simple, but
 elliptical focal spot

 270<sup>0</sup> - small FS, energy accuracy ± 5%, but Bulky

Salalom (112.5<sup>0</sup>) –
 advantages of both ,
 total bending 202.5<sup>0</sup>.





## **Collimation Systems**

Limiting the radiation beamPrimary/fixed collimation

- Cone-shaped, defines maximum field size
- Depleted uranium/Tungsten
- Transmission <0.2%</p>
- Secondary/movable collimator
  - Transmission <2%
  - mounted on either side of the central axis
- Symmetric or asymmetric collimator



# **Multileaf collimators**

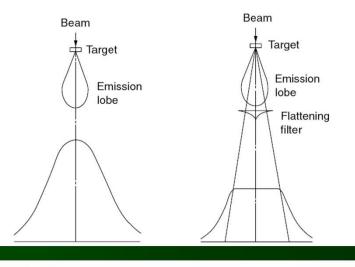
Many independent collimators
Allow irregular field sizes
to be delivered from the linear accelerator.
40–80 pairs of independent collimators
Each leaf has its own motor



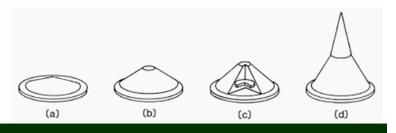
## **Flattening Filter**

#### Conical metal filter

- situated between the target and the ionisation chamber.
- Produce a uniform intensity distribution
- Reduces the output on the central axis of the beam



- •PB Low energies
- •Pb and/or W up to 15 MeV
- •Fe and Pb core 20-25 MeV
- •Al or Fe for higher energies





# Flattening Filter Free Linac

#### **\***Removal of the FF results

- Increase in dose rate (2 4 times higher)
- Softening of the x-ray spectra
- Shift in dmax
- Reduction in head scattered radiation
- Nonuniform beam profile.



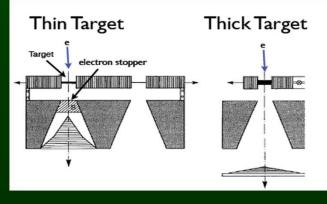
#### X-ray target

#### **\*** X-ray production

- \* up to 10 MeV, a thick tungsten target is employed,
- Thick aluminum target being used for energies greater than this.

#### Retractable for electron beam

therapy.



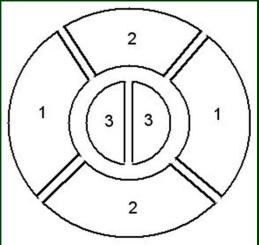




#### **Ionization Chamber**

\* Measures dose & Terminates the beam

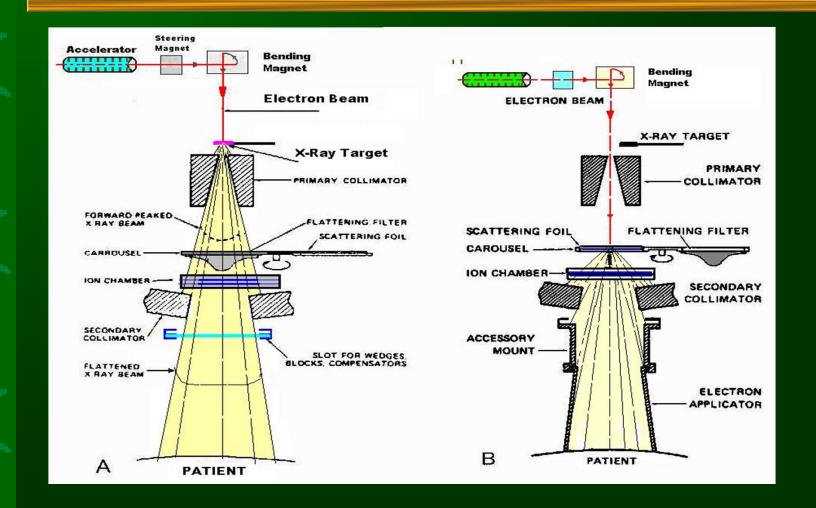
- After prescribed dose
- if the energy, quality, flatness, or dose rate changes
- Two chambers operate independently





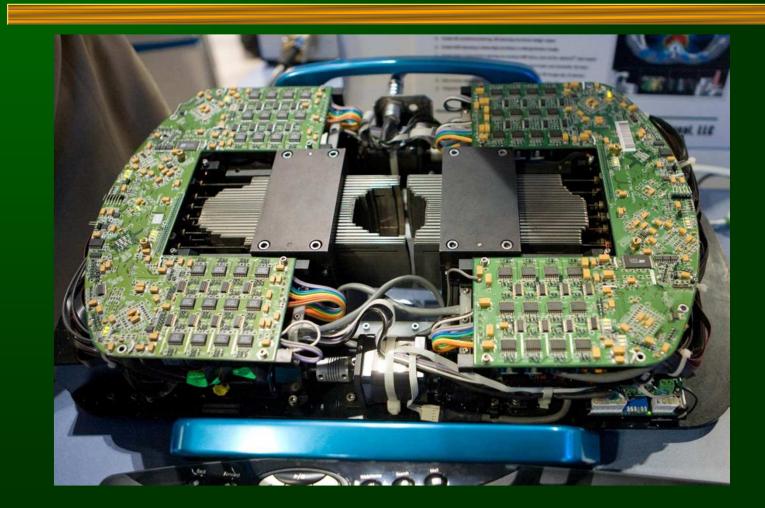


## X-rays & Electron Beam





## MLC



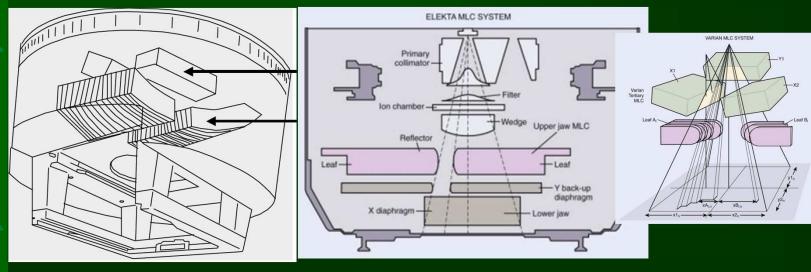


## Types of MLC

#### Three main types

- A Siemens retain upper but replaces lower Jaw
- B Elekta retain lower jaw + backup collimators, replaces upper jaw

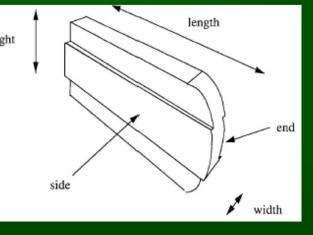
C - Varian - retain all jaws + MLC

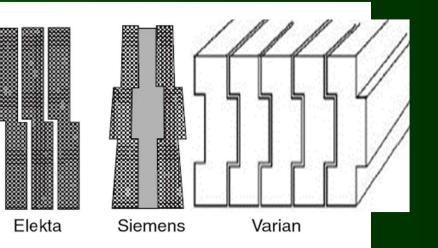




# Comparison

height



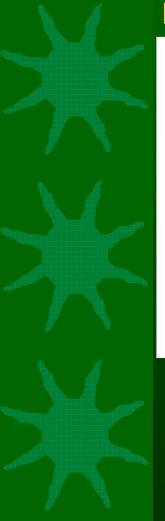


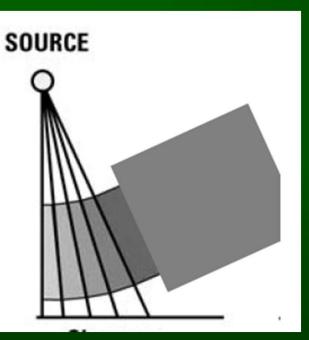
#### Stepped leaves to reduce leakage

	Upper jaw	Lower Jaw	<b>Tertiary</b> Collimator
Elekta	focused MLC	focused block	none
Varian	focused block	focused block	unfocused MLC
Siemens	focused block	focused MLC	none

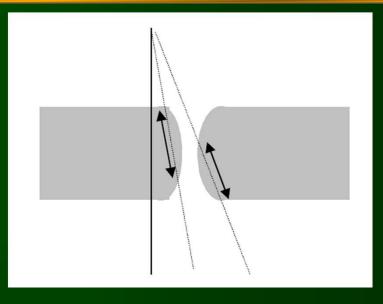


#### **Transmission**





Focused Maintains Divergence



Non-focused, rounded leaf ends The penetration through curved leaves is independent of leaf position.



# **Other facilities**

\* Electron cones
\* Onboard imaging/EPID
\* LASER
\* Optical back pointer
\* Shielding blocks
\* Physical wedges, etc



#### Conclusion

Choice of Equipment
Complex, needs qualified and skilled staff
Constantly developing to the needs of patients
Uptime is high
Require regulated power supply



#### References

- Van Dyk J 1999 Modern Technology of Radiation Oncology vol 1 (Madison, WI: Medical Physics Publishing)
- \* Thwaites *et al* 2006. Back to the future: the history and development of the clinical linear accelerator . *Phys. Med. Biol.* **51** R343-R362
- \* Karzmark C J et al 1993 *Medical Electron Accelerators (New York: McGraw-Hill)*
- Mitzi Baker. Medical linear accelerator celebrates 50 years of treating cancer," Stanford Report, April 18, 2007.
- The History and Role of Accelerators in Radiation Oncology Alfred Smith (University of Texas M.D. Anderson Cancer Center, Houston TX)
- Stanford's medical accelerator, first to treat cancer patients, is on display at Smithsonian," Sandstone & Tile. Vol.2, no.3, p.15.
- The Physics of radiology, 4th edition, Johns, and John
- Sharma SD, Unflattened photon beams from the standard flattening filter free accelerators.....J Med Phys. 2011 Jul-Sep; 36(3): 123–125
- Greene, D., Williams, P.C., Linear Accelerators for Radiation Therapy, Institute of Physics Publishing, Bristol (1997)

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